Comparative evaluation of microtensile bond strength of resin based composite to dentin using an experimental neat-resin dentin bonding agent with ethanol – wet bonding technique – an invitro study

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Introduction

With the introduction of acid etching by Buonocore, a predictable bond strength of 20 – 25 MPa was achieved by enamel bonding to composite resin. However, bonding to dentin posed challenges due to the organic nature and moisture content. This resulted in the evolution of dentin bonding agents [1]. Acid etching and drying the surface resulted in collapse of the collagen fibrils hindering in the penetration of the resin. Therefore, water wet bonding was proposed by Kanca, et al. This technique enabled the penetration of resin into the dentinal collagen resulting in a hybrid layer [2].

The water from the dentin however had to be removed for the penetration of the hydrophobic resin. This led to the development of the etch and rinse adhesives that contained solvents such as ethanol and acetone that acted as water chasers. This also contained a combination of hydrophilic and hydrophobic monomers. The hydrophilic monomers, HEMA, enabled wetting of the bonding agent to the moist dentin and ethanol/ acetone helps in driving away the moisture, subsequently enabling the hydrophobic BIS GMA resin to penetrate the collagen [3].

The water wet bonding and use of etch and rinse system though produced good bonding, they resulted in degradation over time. Two types of degradation results such as hydrolytic degradation and enzymatic degradation. If the moisture is not completely removed from the interphase by the solvents, the hydrophilic monomer HEMA undergoes a hydrolytic degradation due to water sorption. There is also a risk for phase separation of hydrophobic resin (BIS-GMA) from hydrophilic resin monomer. In addition, the host derived matrix metalloproteinases (MMP) gets activated by the etch and rinse systems resulting in degradation of the collagen [4].

To overcome the deleterious effect of residual moisture in water wet bonding and, the use of hydrophilic monomers in the dentin bonding systems, the Ethanol Wet Bonding system was developed. This is based on the histological specimen preparation where ascending grades of alcohol is used to desiccate the tissue specimens. The moist dentin surface is saturated with absolute alcohol to remove the moisture. A hydrophobic resin monomer has been found to effectively bond to this dried surface [5-7]. Use of ascending grades of ethanol was time consuming. Thus a simplified method of using 100% ethanol for 60 seconds have been evaluated [8]. Studies have been done in this concept to assess the bond durability as well as to compare the effect of certain MMP inhibitors with the ethanol wet bonding technique on enzymatic degradation [9-11]. The reports of these studies are promising towards longer durability and MMP inhibition. Studies have been done that assesses the micro tensile bond strength of ethanol wet bonding technique with commercially available dentin bonding agents in enamel, dentin and carious dentin [8,12,13].

This study aims to evaluate the immediate and delayed micro tensile bond strength of the resin composite bonded to dentin with ethanol wet bonding method.

Materials and methodology

This research is an experimental study based on a comparative evaluation of microtensile bond Strength of resin-based composite to dentin using an experimental neat-resin dentin bonding agent with ethanol – wet bonding technique – An Invitro study. Sample preparation were done in Department of Conservative Dentistry & Endodontics, IGIDS, Pondicherry and Bond strength was evaluated by using universal testing machine in CIPET (Central Institute of Plastic and Engineering Technology), Guindy, Chennai.

The study was approved by the Institutional review board on 01.12.2016 Ref no – IGIDSIRB2016NDP12PGNDCDE and Institutional Ethical committee on 16.12.16 Ref no – IGIDSIEC2016NDP12PGNDCDE

Non carious extracted third molars were collected in IGIDS, Puducherry which fulfilled the inclusion and exclusion criteria were selected. The following inclusion criteria were used for tooth sample collection: Freshly extracted impacted mandibular third molar, Without carious lesions, Without cracks or fractures during extraction procedure. Carious/ non-carious lesions/ traumatic fractures if present, the teeth are excluded.

40 freshly extracted third molars were used in this study. The sample size was determined in the pilot study by using mean and standard deviation and found to be 40.

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The samples were divided into two groups and each group were divided into two subgroups in which each subgroup will contain 10 samples. Each tooth can yield 10 composite-resin beam of 1x1x6mm³. Equals to 100 beams per subgroup.

Sample size calculated with mean and SD of micro tensile bond strength in MPa obtained from Sadek, et al for the subgroup of 24 hours microtensile bond strength [14]. Sample size calculated with G* Power 3.1.9.2, Germany. Samples calculated was 95 per subgroup. Approximated to 100 per subgroup after accounting for 10% sample loss.

Forty freshly extracted, intact, non-carious, impacted third molars were cleaned and stored in distilled water. Informed consent was obtained from the patients before extraction.

Sample preparation

The roots were resected at the cervical region with the diamond disc under water coolant. The clinical crown was trimmed below the CEJ, with the diamond disc under water coolant, exposing a flat middle dentinal surface. The teeth was fixed to an acrylic block with cyanoacrylate resin. 180 grit silicon carbide paper was used to polish the surface to create a dentinal smear layer [11].

Sample allocation

Samples were divided into two groups (n=20) per group. Group 1: ethanol wet bonding method primed with 50wt % of experimental neat resin monomer and 50 wt % of absolute ethanol bonded with neat monomer. Group 2: water wet bonding method primed and bonded with ethanol based etch and rinse adhesive (3M Adper single Bond 2)

Preparation of experimental neat resin

A co-monomer resin was prepared consisting of the following composition will be made 70%wt bisphenol A diglycidyletherdimethacrylate (BIS-GMA) (SIGMA-ALDRICH) 28.75% tetra-ethylene glycol dimethacrylate (TEGDMA) (SIGMA-ALDRICH) 0.25% Camphorquinone (CQ) (SIGMA-ALDRICH) 1wt% ethyl N, N-4 aminobenzoate (SIGMA-ALDRICH)

Priming and bonding procedure

All samples in both groups were acid etched with 35% phosphoric acid for 15 sec.

They were washed with distilled water. Blot dried with absorbent paper leaving the surface moist.

Group 1: bonding of resin composite in ethanol wet bonding (n=20)

The dentin surface was inverted in 2ml of 100%ethanol for 60 sec (saturating the dentin with ethanol).

Excess ethanol was blot dried with absorbent paper 50 wt% neat resin and 50wt% absolute ethanol was applied to the dentin with fine microbrush in two thin coats and are agitated for 10 secs. The excess primer was evaporated with a chip blower for 10 secs. Experimental neat resin monomer was applied in the surface as an adhesive.

Light curing was done with LED curing at 600mw/cm². Resin composite (3M3SPF Filtek Z350 XT) build up was done in 2mm. increments in two increment to a height of 4mm. (fig 15). Each layer was light cured for 40 secs. Each tooth was sectioned into 1x1x6mm³ sized composite-dentin beam by non-trimming method. Samples were stored in artificial saliva.

Group 2: bonding of resin composite in water wet bonding method (n=20)

Application of etch and rinse ethanol-based dentin bonding agent, 3M ADPER Single Bond 2, as per manufacturers instrumentation, to the etched, rinsed and blot dried dentin surface. Composite resin build up as mentioned in groups 1 will be done. Sectioned teeth were stored in artificial saliva as in group 1.

Preparation of artificial saliva

The artificial saliva is prepared by mixing CaCl₂, (0.7)-calcium chloride, MgCl₂.6H₂O (0.2), KH₂PO₄(4.0), KCl (30), NaCl,(0.3), HEPES buffer. (4-(2hydroxyethyl)-1-piperazineethane sulfonic acid). The samples are stored in this at 37°C. The solution is changed periodically.

Microtensile bond strength testing

Both groups 1 and 2 were subdivided into two groups:

- sub group 1a: for immediate micro tensile bond strength evaluation (n=10)
- subgroup 1b: for micro tensile bond strength evaluation after nine months of storage (n=10)
- Group 2: sub group 2a: for immediate micro tensile bond strength evaluation (n=10)
- subgroup 2b: for micro tensile bond strength evaluation after nine months of storage (n=10).

Each tooth was sectioned into 1x1x6mm³ sized composite-dentin beam by non-trimming method. Ten beams from each tooth were selected for micro tensile bond strength. The beams were attached to the test apparatus with cyanoacrylate adhesive.

The beams were stressed to fail under tension using a universal testing machine at a constant cross head speed of 1mm/min. Fractographical analysis was made under SEM (adhesive/cohesive/or mixed failure). Bond strength values were measured in MPa.

Statistical methods

Descriptive Statistics: Mean and SD of the micro tensile bond strength in MPa. (Table 1 and 2)

According to the statistical analysis paired t test were used

STD.DEVATION = WWB -24 hrs-3.0315

EWB -24 hrs-5.5613

WWB -9 months -1.4824

EWB 9 months -2.4097

After bond strength testing the samples were air dried, sputter coated with gold palladium and were seen under SEM, failure mode was identified. The microtensile bond strength values of water wet bonding and ethanol bonding. Control group 40 samples 400 samples were obtained in MPa n=400

In WWB condition: For group 1 a control group, WWB-24 mean score is 21.46±3.03 MPa WWB -9 months is 18.81±1.45 MPa

In EWB group -Group 2 a -EWB-24 hrs mean is 54.47±5.56 MPa, EWB 9 months 40.8773±2.40 MPa

Inferential statistics:

Paired t test is used to determine if there was difference between WWB and EWB 24 hrs bond strength for both

WWB and EWB showed a mean value of -33.011±6.56 MPa

9 months showed -22.064±2.85 MPa (p>0.005) – 3
Table 1. Bond strength values in Mpa

<table>
<thead>
<tr>
<th>Paired Samples Test</th>
<th>Mean</th>
<th>N</th>
<th>Std. Deviation</th>
<th>Std. Error Mean</th>
</tr>
</thead>
<tbody>
<tr>
<td>Pair 1 WWB24</td>
<td>21.46037</td>
<td>100</td>
<td>3.031559</td>
<td>0.303156</td>
</tr>
<tr>
<td>EWB24</td>
<td>54.47212</td>
<td>100</td>
<td>5.563151</td>
<td>0.556315</td>
</tr>
<tr>
<td>Pair 2 WWB9M</td>
<td>18.8125</td>
<td>100</td>
<td>1.48246</td>
<td>0.14825</td>
</tr>
<tr>
<td>EWB9M</td>
<td>40.8773</td>
<td>100</td>
<td>2.40979</td>
<td>0.24098</td>
</tr>
</tbody>
</table>

Table 2. Paired samples test

<table>
<thead>
<tr>
<th>Paired Differences</th>
<th>Mean</th>
<th>Std. Deviation</th>
<th>Std. Error Mean</th>
<th>95% Confidence Interval of the Difference</th>
<th>Lower</th>
<th>Upper</th>
<th>t</th>
<th>df</th>
<th>Sig. (2tailed)</th>
</tr>
</thead>
<tbody>
<tr>
<td>Pair 1 WWB24-EWB24</td>
<td>-33.01175</td>
<td>6.566197</td>
<td>0.656620</td>
<td>-34.314626</td>
<td>-32.708874</td>
<td>-30.275</td>
<td>99</td>
<td>0.000</td>
<td></td>
</tr>
<tr>
<td>Pair 2 WWB9M-EWB9M</td>
<td>-22.06477</td>
<td>2.85068</td>
<td>0.28507</td>
<td>-22.63041</td>
<td>-21.49913</td>
<td>-21.77402</td>
<td>99</td>
<td>0.000</td>
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</tr>
</tbody>
</table>

Discussion

The seek for an artificial restorative material mimicking natural tooth both in function and aesthetics in the oral environment still remains a primary concern to the dentist which has led to the use of a number of restorative materials in dentistry. The science and technology of composite dental restorative materials have progressed significantly over the past 10 years. The concept of composite and bonding to tooth structure has led to major alterations in cavity preparation, with a general drift towards the increased preservation of healthy, natural tooth structure. In spite of the significant improvements in adhesive systems, the bonded interface remains the weakest area of composite restorations.

Due to complex chemico micromechanical bonding current composite materials fail to resist the effects of marginal penetration and the leakage of oral fluids as enamel has less than 1.00% of water content, hydrophobic resin worked well as long as they were restricted only to enamel. Dentin consists of 50% volume of inorganic material 30% of organic and 20% volume of fluids. After acid etching, the demineralized dentin consists of 30% of collagen and 70% water [15]. Whenever a resin infiltrated dentin between the adhesive and non-demineralized fibres in demineralized dentin to form a hybrid layer consisting of resin infiltrated dentin between the adhesive and non-demineralized dentin. Initially during etch and rinse technique when etched dentin is dried using air way syringe bond strength is decreased because of the Collapse of collagen fibres. When water is removed, the collagen with fewer intrafibrillar spaces open for the penetration of the monomers. This dehydration permits additional hydrogen bonds to form between collagen, leaving no interfibrillar a space which results in decreased bond strength. The interfibrillar spaces can be expanded by refilling with water. In the early 1990s “wet” or moist bonding, technique was developed by Kanca to improve initial bond strength of etch and rinse adhesive. In this technique water is used as a solvent which permits to re expand the collapsed demineralized dentin matrices prior to resin infiltration, but water is not a proper solvent for resin monomer as resin monomers miscibility is limited in the water, resulting in the phase separation of hydrophobic resin [18]. The excess water causes sub optimal polymerization, nanoleakage and activation of matrix metallocproteinase which may all lead to biodegradation of resin dentin interface [2].

The use of adhesives on moist dentin is made possible by incorporation of organic solvents acetone or ethanol in the primer or adhesive, since these solvents displace water from the dentin surface and promotes the infiltration of resin monomer through the nanospaces of dense collagen web [16,19].

The hydrophilic nature of the adhesive resin absorbs water leading to the plasticization effect reducing the mechanical properties of the resin component of adhesive joint To overcome the drawbacks of WWB and hydrophilic resin, EWB and hydrophobic resins were introduced by Tay, et al. Ethanol a water-based solvent used to support the demineralized dentin collagen fibrils and facilitate the penetration of BISGMA a hydrophobic adhesive resin into the ethanol saturated demineralized dentin. Ethanol saturated demineralized dentin matrices can be achieved by treating acid etched dentin surfaces with a series of increasing ethanol concentration (50, 70, 80, 95, and 100% 3 times each, for 30 s), for 3–4 min. As this process was tedious and time consuming, 100% ethanol for 1 min can be used which is called as “simplified ethanol wet bonding technique”. This technique also can replace water while maintaining the collagen fibrils and promotes infiltration of resin monomers. When ethanol is mixed with the hydrophobic resin there is formation of hydrogen bonds between water and ethanol molecules which leads to better evaporation of water ethanol aggregate than plain water [10]. The principles of ethanol-wet-bonding are explained by using Hoy’s triple solubility parameter theory [12].

The Solubility parameters for hydrogen bonding forces (δh) can predict the nature of any solvents or resin’s capability to re-expand a collapsed dried acid etched dentin. When demineralized dentin matrices are collapsed (dried dentin), to re expand matrices again, a solvent or resin monomer should have a higher hydrogen bonding force of more than 14.8 (J/cm³) when ethanol was used as a substitute to rinse water from acid-etched matrices, the collapse of matrices was very less and resin infiltration into the hybrid layer appeared to be very high. But acetone has only 11 (J/cm³) which is not sufficient to cleave the interpeptide hydrogen bonding between the collagen fibrils. Later investigations confirmed that ethanol wet-bonding enhances resin infiltration which promotes higher penetration and bonding of resin to the tooth surface in comparison with conventional water wetbonding [12].

The rationale behind microtensile bond strength testing method is that the stronger the adhesion between tooth and biomaterial, the better it will resist stress imposed by resin polymerization and oral function.
The samples of group 1(EWB)-1a,1b, group 2 (WWB)-2a,2b were etched and the groups 1a,1b were saturated in 100%ethanol for 60 sec and blot dried. Two coats of the experimental neat resin are applied on to the ethanol saturated demineralized dentin surface. The experimental neat resin is prepared based on is used in group 1 [11]. In group 2a,2b ethanol based etch and rinse adhesive (3M Adaper single Bond 2) is used which consists of HEMA, BISGMA, Fillers, Ethanol, water, initiators. Resin composite build ups were done using (3M3SP Filtek Z350 XT) made of BISGMA, UDMA, BISEMA-6, minimum amount of TEGDMA, Silica and light cured. Resin composite build ups were done using (3M3SP Filtek Z350 XT) made of BISGMA, UDMA, BISEMA-6, minimum amount of TEGDMA, Silica and light cured. Resin composite build ups were done using (3M3SP Filtek Z350 XT) made of BISGMA, UDMA, BISEMA-6, minimum amount of TEGDMA, Silica and light cured. In group 2a,2b ethanol based etch and rinse adhesive (3M Adaper single Bond 2) is used which consists of HEMA, BISGMA, Fillers, Ethanol, water, initiators. Resin composite build ups were done using (3M3SP Filtek Z350 XT) made of BISGMA, UDMA, BISEMA-6, minimum amount of TEGDMA, Silica and light cured. Resin composite build ups were done using (3M3SP Filtek Z350 XT) made of BISGMA, UDMA, BISEMA-6, minimum amount of TEGDMA, Silica and light cured.

Microtensile bond strength was tested in a universal testing machine (INSTRON) in CIPET Guidy Chennai. Only group 1a, 2a is tested to check immediate bond strength the other groups 1b, 2b were immersed in artificial saliva for a period of nine months.

A separate fixture was made to grasp the beam sticks and the fixture is held on to the UTM machine in which the sticks were bonded to the test apparatus with cyanoacrylate resin. The sticks were held with the tweezer. These beams were stressed to fail under tension at a constant cross head speed of about 1mm/min until the sticks break and that particular point where the fracture occurred the values were noted in MPa. All the fractured sticks were collected and placed separately and were coated with gold sputtering nanoparticles and later representative samples from each group was observed under scanning electron microscope to identify what type of fracture it is (adhesive, cohesive or mixed failure). SEM scans the surface of the samples with a focused beam of electrons and produces an image. Fractographical analysis were made. The samples of EWB showed fracture extending from the adhesive to composite or to dentin (mixed failures) while WWB group showed entirely between adhesive and dentin (adhesive failure). (Figures 1a,1b and 2)

According to the statistical analysis paired t test were used

For WWB (24hrs)-immediate bond strength values were 21.460; WWB-9 months -18.8125, EWB- immediate bond strength values were-54.47; EWB-9 months-40.877

Std.deviation –WWB 24 hrs-3.0315; WWB-9 months-1.4824, EWB-24hrs-5.5613; EWB 9 months -2.4097. There showed a decrease in bond strength after 9 months of storage in artificial saliva.

![SEM-GROUP 1a IMMEDIATE MTBS](image1.png)

![SEM-GROUP 1b NINE MONTHS](image2.png)

**Figure 1a,1b.** Mean ethanol wet bonding strength recorded among the groups

![ETHANOL WET BONDING](image3.png)

![WATER WET BONDING](image4.png)

**Figure 2.** Mean water wet bonding strength recorded among the groups
Conclusion

The simplified ethanol wet bonding technique shows improved microtensile bond strength in sound dentin. The advantage of the ethanol-wet bonding technique is that it can effectively allow less hydrophobic monomers into the dentine matrix, creating a more hydrophobic hybrid layer that could absorb less water over time. Thus ethanol wet bonding group1 showed better bonding than water wet bonding group 2.

References